

Case Report

Adverse Reactions to Metal Debris after Fully-Modular Primary Total Hip Arthroplasty: A Report of Two Cases

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Abstract

Adverse reactions to metal debris (ARMDs) are a current concern in total hip arthroplasty (THA). The occurrence of ARMDs is well documented in metal-on-metal (MoM) resurfacing and THA and corrosion at a modular neck-body junction with a metal-on-polyethylene (MoP) bearing THA has recently been reported. However, dual-modular primary THA including modular stem-neck and neck-head junctions is not well documented. We performed 18 MoP THAs with a 40-mm diameter head (2011-2016), and two patients required revision arthroplasty for a symptomatic pseudotumor with corrosion, at the modular head-neck junction in one and at the neck-body junction in the other.

INTRODUCTION

Adverse reactions to metal debris (ARMDs) are a current concern in total hip arthroplasty (THA) [1-4]. They encompass a wide spectrum of pathological conditions associated with metal ion release [5], including fluid collection, aseptic lymphocytic vasculitis-associated lesions (ALVALs), tissue necrosis [6], and pseudotumor formation [7,8]. The occurrence of ARMDs is well documented in metal-on-metal (MoM) resurfacing and THA [1,9,10]. An adverse local tissue reaction (ALTR) can occur in patients with a metal-on-polyethylene (MoP) bearing secondary to corrosion at the modular femoral head-neck junction, and their presentation is similar to the ALTRs seen in patients with a MoM bearing [11,12]. The occurrence of corrosion at a modular neck-body junction with a MoP bearing THA has recently been reported [2,5,11,13]. However, dual-modular primary THA including modular stem-neck and neck-head junctions is not well documented [14-16].

Between 2011 and 2016, we performed 18 MoP THAs with a 40-mm diameter head, and two patients required revision arthroplasty for a symptomatic pseudotumor. The present report describes the clinical presentation, diagnosis, and early results of operative treatment of patients with corrosion, at the modular head-neck junction in Case 1 and at the neck-body junction in Case 2, of MoP THAs. The patients gave their informed consent prior to their inclusion in this study. This study was reviewed by

the institutional ethics committee and was therefore performed in accordance with the ethical standards laid down in the latest version of the 1964 Declaration of Helsinki.

CASE REPORTS**Case 1**

A 49-year-old woman (weight 72 kg, height 156 cm) underwent an uncemented right THA for osteoarthritis of the hip (acetabular implant, 54-mm Trident® acetabular cup (pure titanium) with X3® ultra-high molecular weight cross-linked polyethylene (UHMWXP) insert of 5.8 mm thickness (Stryker Orthopaedics, Mahwah, NJ); femoral implant, Pro femur Z® femoral stem (Ti, 6Al, 4V) with a 4.5° anteverted and 6° varus neck (Ti, 6Al, 4V), and a 40-mm Conserve Plus® short head (Co-Cr alloy) (Wright Medical Technology; Arlington, TN)) (Figure 1). She was reviewed 2 years later and found to have no pain, a normal range of hip motion, and able to fully weight-bear without supporting aids, but she had a clicking and clunking sensation during index hip flexion moment 23 months postoperatively. At the same time, she noticed a soft tissue mass in her right inguinal region.

Inflammatory serology was normal. The serum cobalt and chromium ion levels were 2.4 ng/ml and 0.05 ng/ml, respectively. Plain radiographs did not show any impending implant failure, but calcar osteolysis was visible (Figure 1). An ultrasound scan

(APLIO XG SSA-790A PLT-805AT, Toshiba Medical Systems Corp., Tokyo, Japan) showed a mixed fluid and solid mass (Figure 2). Magnetic resonance imaging (MRI) (Signa HDxt 1.5T Optima Edition GE Healthcare, Tokyo, Japan) demonstrated a large pseudotumor around the anterior hip joint (Figure 3). Diagnosed as ARMD, she underwent revision surgery. A large amount of abnormal fluid, ranging from milky white to yellow in color (Figure 4), was encountered on incising the tensor iliotibial band through a posterolateral approach. Metal concentrations of the joint fluid were Co 640 ng/ml and Cr 100 ng/ml. Intraoperative cultures were negative. Hypertrophy of the synovial tissue and a huge pseudocapsule were noted and completely resected. The femoral head-neck junction demonstrated obvious corrosion (Figure 4). The modular neck and femoral components were well-fixed. The 40-mm metal head, neck, and stem were replaced with a 32-mm delta ceramic head BIOLOX® (CeramTec AG, Plochingen, Germany) and Profemur R® stem (Ti, 6Al, 4V). Histological examination showed peri vascular lymphocyte infiltration, necrotic tissue, and giant cells (Figure 5).

Case 2

A 69-year-old woman (weight 47 kg, height 144 cm, at initial surgery) underwent a right uncemented THA for osteoarthritis of the hip. The posterolateral surgical approach for THA was

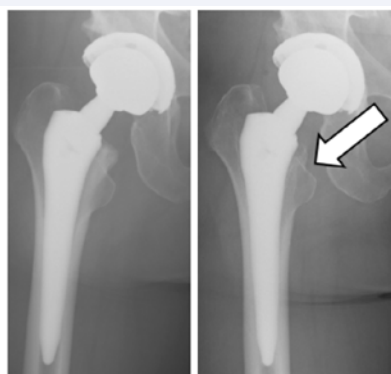


Figure 1 Immediate postoperative antero posterior radiograph of the hip at primary THA (A) and 2 years after surgery (B) showing calcar resorption (arrow).

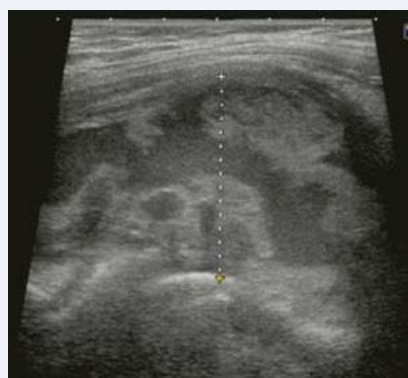


Figure 2 Ultrasound scan, lateral to anterior, of the hip in Case 1, demonstrating a mixed fluid and solid mass.



Figure 3 T2-weighted coronal MR image in Case 1 (Arrow: pseudotumor).

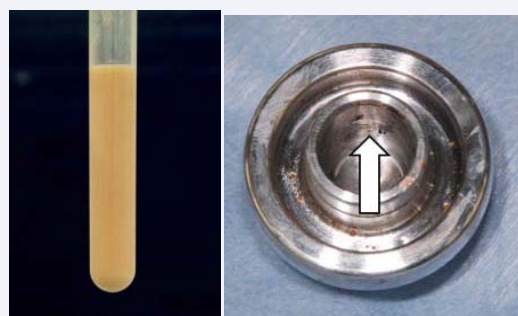


Figure 4 Dark yellowish turbid fluid in the hip of Case 1 (A). Black deposits containing corrosion products are visible at the head taper (B).

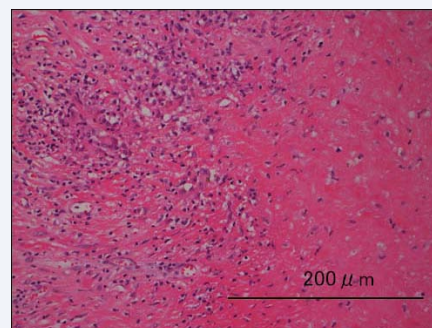


Figure 5 Pathological specimen in Case 1 (hematoxylin and eosin, ×20). See text.

used to implant a 52-mm Trident® acetabular cup with a 3.8-mm thick X3® UHMWXP insert, a Profemur Z® femoral stem with a 4.5° retroverted and 6° varus neck, and a 40-mm Conserve Plus® medium metal head (Figure 6). Two months after surgery, she felt discomfort around the right hip joint, but no pain. Although she had a normal range of hip motion, she felt difficulty when she lifted her right leg, and needed a cane to walk. The symptoms continued up to revision surgery. Inflammatory serology was normal. Plain radiographs did not show any impending implant failure, but calcar osteolysis was visible 3 years after implantation (Figure 6). An ultrasound scan showed fluid collection around the hip joint. MRI demonstrated a large pseudotumor around the hip joint (Figure 7). Diagnosed as ARMD, revision surgery was performed.

A large amount of yellowish translucent fluid was encountered by section of the iliopsoas tendon through a posterolateral approach. Intraoperative cultures were negative. Hypertrophied synovial tissue and a large pseudo capsule were present in the posterior hip, with proximal femoral cortical thinning. The neck-stem junction, but not the femoral head-neck junction, demonstrated obvious corrosion and wear debris (Figure 8). The modular neck and femoral components were well-fixed. The implants were replaced with a 36-mm delta ceramic head (BIOLOX®) and Profemur-R® stem with a modular neck. Metal concentrations of the joint fluid were cobalt 3 ng/ml and chromium 32 ng/ml. Pathology was similar to that of Case 1 (Figure 9).

DISCUSSION

The head-neck junction and the modular neck-stem junction have been reported to have mechanical and chemical problems [17-19]. In the trunnion, where the neck and head junction tapers, micromotion occurs and body fluids penetrate into this junction, facilitating mechanically assisted crevice and fretting corrosion [18,19]. Micromotion increases corrosion rates, because oxide layers are continually fractured and reformed (repassivation) on the metallic surface [19]. Larger head size causes more fretting and corrosion in the MoP system [3]. Hallab et al. [19], also showed that fretting and voltage change, as well as metal release,

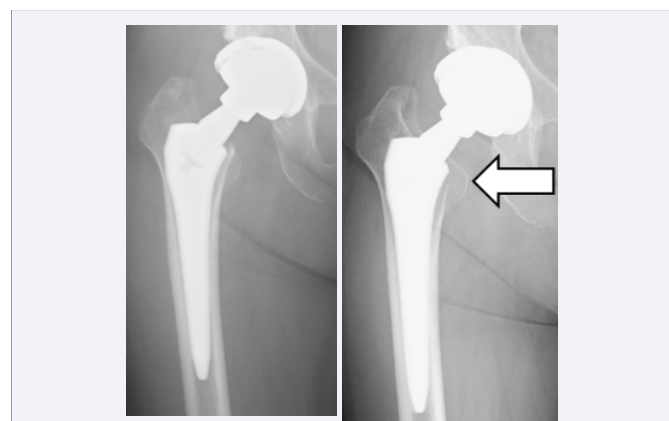


Figure 6 Immediate postoperative anteroposterior radiograph of the hip (A), and 3 years after surgery (B) (arrow: osteolysis).



Figure 7 Ultrasound scan around the hip in Case 2 demonstrating a low echoic mass.



Figure 8 T2-weighted coronal MR image in Case 2 shows a pseudo tumor (arrow).

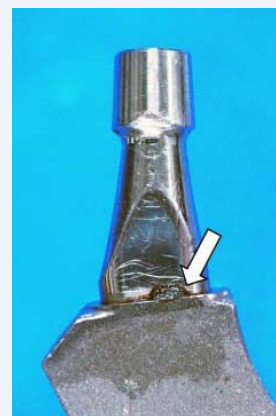


Figure 9 Corrosion of the neck-body junction (arrow) in Case 2.

were greater in a metal head than in a ceramic head with a Co-Cr alloy head system. In our system, the titanium neck and Co-Cr alloy head generated galvanic corrosion, which was defined as an electrochemical interaction between dissimilar metals that results in a flow of electrons between them [18]. Early failure has also been reported previously [2,11,13,14]. The present two cases developed corrosion at the modular femoral head-neck junction (Case 1) and neck-stem junction (Case 2) of a dissimilar head-neck system with a MoP bearing [2,16]. A previous study suggested that with a similar metal combination, crevice, stress, and motion had less of an effect [20]. The above-mentioned fretting and galvanic corrosion and the large head size also led to early revision [21]. Recent advancements in polyethylene liner head size in MoP THA [22] are not related to early revision compared to Mo M THA [23].

These fully-modular necks (modular head-neck and neck-stem junctions) allows us to more restore patient anatomy, such as limb length, lateral offset, muscle balance, and femoral anteversion to prevent dislocation. However, modularity also increased the number of mechanical junctions that may lead to above mentioned corrosions and then catastrophic fractures [24,25]. Fokter et al., reviewed 13 cases of fully-modular necks

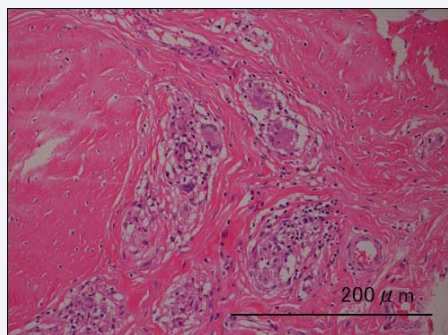


Figure 10 Pathological specimen of Case 2 (hematoxylin and eosin, $\times 20$). See text.

[25]. Most patients were heavy weights and high body mass indexes, those of our cases were 72 and 47 kg, 29.6 and 24.6 kg/m², respectively. The lighter body weights may not induce neck fracture.

ARMD was reported in late 2000 in MoM hip resurfacing [1,26]. Pseudotumors were also reported in late 2000 with the same systems [8]. These reactions were investigated as hypersensitivity to metals [6]. Histomorphological study showed an aseptic lymphocytic-dominant vasculitis-associated lesion (ALVAL), as shown in Figure (5) and Figure (10).

To identify these reactions, a specialized metal artifact reduction sequence (MARS) MRI has been recommended [26]. However, our institution was not equipped with this expensive system, and diagnostic ultrasonography was chosen as a screening tool instead [4,27,28]. As shown in Figure (2) and Figure (7), the latter tool was economical and cost-effective compared to MRI [29]. For arthrocentesis, it was easy to demonstrate the area of fluid collection. Finally, ceramic heads were used for revision surgery. This procedure was supported by several reports [19,26,30]. Goyal et al., reported good results of THA with adverse local tissue reactions by a ball (Co-Cr alloy) and liner exchange without stem (Co-Cr alloy) revision [31]. However, we chose ceramic heads for the newly implanted Profemur-R® stems and modular necks.

REFERENCES

- Langton DJ, Jameson SS, Joyce TJ, Hallab NJ, Natsu S, Nargol AV. Early failure of metal-on-metal bearings in hip resurfacing and large-diameter total hip replacement: A consequence of excess wear. *J Bone Joint Surg Br.* 2010; 92: 38-46.
- Whitehouse MR, Endo M, Zachara S, Nielsen TO, Greidanus NV, Masri BA, et al. Adverse local tissue reactions in metal-on-polyethylene total hip arthroplasty due to trunnion corrosion: the risk of misdiagnosis. *Bone Joint J.* 2015; 97: 1024-1030.
- Raju S, Chinnakkannu K, Puttaswamy MK, Phillips MJ. Trunnion Corrosion in Metal-on-Polyethylene Total Hip Arthroplasty: A Case Series. *J Am Acad Orthop Surg.* 2017; 25: 133-139.
- Kwon Y-M, Lombardi AV, Jacobs JJ, Fehring TK, Lewis CG, Cabanela ME. Risk stratification algorithm for management of patients with metal-on-metal hip arthroplasty. Consensus statement of the American Association of Hip and Knee Surgeons, the American Academy of Orthopaedic Surgeons, and the Hip Society. *J Bone Joint Surg Am.* 2014; 96.
- Shulman RM, Zywielski MG, Gandhi R, Davey JR, Salonen DC. Trunnionosis: the latest culprit in adverse reactions to metal debris following hip arthroplasty. *Skeletal Radiol.* 2015; 44: 433-440.
- Willert HG, Buchhorn GH, Fayyazi A, Flury R, Windler M, Köster G, et al. Metal-on-metal bearings and hypersensitivity in patients with artificial hip joints. A clinical and histomorphological study. *J Bone Joint Surg Am.* 2005; 87: 28-36.
- Kiran M, Boscainos PJ. Adverse reactions to metal debris in metal-on-polyethylene total hip arthroplasty using a titanium-molybdenum-zirconium-iron alloy stem. *J Arthroplasty.* 2015; 30: 277-2281.
- Pandit H, Glyn-Jones S, McLardy-Smith P, Gundle R, Whitwell D, Gibbons CL, et al. Pseudotumours associated with metal-on-metal hip resurfacings. *J Bone Joint Surg Br.* 2008; 90: 847-851.
- Hart AJ, Satchithananda K, Liddle AD, Sabah SA, McRobbie D, Henckel J, et al. Pseudotumors in association with well-functioning metal-on-metal hip prostheses. A case-control study using three-dimensional computed tomography and magnetic resonance imaging. *J Bone Joint Surg Am.* 2012; 94: 317-325.
- Hart AJ, Sabah SA, Bandi AS, Maggiore P, Tarassoli P, Sampson B, et al. Sensitivity and specificity of blood cobalt and chromium metal ions for predicting failure of metal-on-metal hip replacement. *J Bone Joint Surg Br.* 2011; 93: 1308-1313.
- Cooper HJ, Della Valle CJ, Berger RA, Tetreault M, Paprosky WG, Sporer SM, et al. Corrosion at the head-neck taper as a cause for adverse local tissue reactions after total hip arthroplasty. *J Bone Joint Surg Am.* 2012; 94: 1655-1661.
- Lindgren JU, Brismar BH, Wikström AC. Adverse reaction to metal release from a modular metal-on-polyethylene hip prosthesis. *J Bone Joint Surg Br.* 2011; 93: 1427-1430.
- Cooper HJ, Urban RM, Wixson RL, Meneghini RM, Jacobs JJ. Adverse local tissue reaction arising from corrosion at the femoral neck-body junction in a dual-taper stem with a cobalt-chromium modular neck. *J Bone Joint Surg Am.* 2013; 95: 865-872.
- Molloy DO, Munir S, Jack CM, Cross MB, Walter WL, Walter WK Sr. Fretting and corrosion in modular-neck total hip arthroplasty femoral stems. *J Bone Joint Surg Am.* 2014; 96: 488-493.
- Gill IP, Webb J, Sloan K, Beaver RJ. Corrosion at the neck-stem junction as a cause of metal ion release and pseudotumour formation. *J Bone Joint Surg Br.* 2012; 94: 895-900.
- Silverton CD, Jacobs JJ, Devitt JW, Cooper HJ. Midterm results of a femoral stem with a modular neck design: clinical outcomes and metal ion analysis. *J Arthroplasty.* 2014; 29: 1768-1773.
- Collier JP, Surprenant VA, Jensen RE, Mayor MB, Surprenant HP. Corrosion between the components of modular femoral hip prostheses. *J Bone Joint Surg Br.* 1992; 74: 511-517.
- Jacobs JJ, Gilbert JL, Urban RM. Corrosion of metal orthopaedic implants. *J Bone Joint Surg Am.* 1998; 80: 268-282.
- Hallab NJ, Messina C, Skipor A, Jacobs JJ. Differences in the fretting corrosion of metal-metal and ceramic-metal modular junctions of total hip replacements. *J Orthop Res.* 2004; 22: 250-259.
- Gilbert JL, Buckley CA, Jacobs JJ. In vivo corrosion of modular hip prosthesis components in mixed and similar metal combinations. The effects of crevice, stress, motion, and alloy co. *J Biomed Mater Res.* 1993; 27: 1533-1544.
- Elkins JM, Callaghan JJ, Brown TD. Stability and trunnion wear potential in large-diameter metal-on-metal total hips: a finite element analysis. *Clin Orthop Relat Res.* 2014; 472: 529-542.
- Triantafyllopoulos GK, Elpers ME, Burket JC, Esposito CI, Padgett

- DE, Wright TM. Otto Aufranc Award: Large heads do not increase damage at the head-neck taper of metal-on-polyethylene total hip arthroplasties. *Clin Orthop Relat Res* 2016; 474: 330-338.
23. Bishop NE, Hothan A, Morlock MM. High friction moments in large hard-on-hard hip replacement bearings in conditions of poor lubrication. *J Orthop Res*. 2013; 31: 807-813.
24. Fokter SK, Moličnik A, Kavalari R, Pelicon P, Rudolf R, Gubeljak N6. Why do some titanium-alloy total hip arthroplasty modular necks fail? *J Mech Behav Biomed Mater*. 2016; 69: 107-114.
25. Fokter SK, Rudolf R, Moličnik A. Titanium alloy femoral neck fracture-clinical and metallurgical analysis in 6 cases. *Acta Orthop*. 2016; 87: 197-202.
26. Bolognesi MP, Ledford CK. Metal-on-Metal Total Hip Arthroplasty: Patient Evaluation and Treatment. *J Am Acad Orthop Surg*. 2015; 23: 724-731.
27. Garbuz DS, Hargreaves BA, Duncan CP, Masri BA, Wilson DR, Forster BB. The John Charnley Award. Diagnostic accuracy of MRI versus ultrasound for detecting pseudotumors in asymptomatic metal-on-meal THA. *Clin Orthop Relat Res*. 2014; 472: 417-423.
28. Nishii T, Sakai T, Takao M, Yoshikawa H, Sugano N. Ultrasound screening of periarticular soft tissue abnormality around metal-on-metal bearings. *J Arthroplasty*. 2012; 27: 895-900.
29. Glyn-Jones S, McLardy-Smith P, Gill HS, Murray DW. The creep and wear of highly cross-linked polyethylene. A three-year randomized, controlled trial using radiostereometric analysis. *J Bone Joint Surg Br*. 2008; 90: 556-561.
30. Kurtz SM, Kocagöz SB, Hanzlik JA, Underwood RJ, Gilbert JL, MacDonald DW, et al. Do ceramic femoral heads reduce taper fretting corrosion in hip arthroplasty? A retrieval study. *Clin Orthop Relat Res*. 2013; 471: 3270-3282.
31. Goyal N, Ho H2, Fricka KB, Engh CA Jr1. Do you have to remove a corroded femoral stem? *J Arthroplasty*. 2014; 29: 139-142.

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