

Review Article

The Diurnal Variation “accordion”-like Phenomenon of Wedged Intervertebral Discs: A Progression Factor in Idiopathic Scoliosis

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Abstract

This report presents a concept for idiopathic scoliosis (IS) progression, which refers to the role of the diurnal variation on the asymmetric water distribution of the eccentric nucleus pulposus of the deformed scoliotic IVD, and the subsequent alteration of the mechanical environment, due to caused intermittent forces, on the adjacent vertebral growth plates. The result of these intermittent forces, due to the diurnal variation, is an asymmetrical vertebral growth and progression of the deformity. This is termed the “accordion-like phenomenon”.

It concisely discusses data used to lend support to the presented concept, relate to the mechanobiology, the mechanotransduction process, and fundamentals of the embryology and biology of the spinal column. It also relates to the normal and deformed intervertebral disc, the diurnal variation phenomenon, concepts of IS scoliogeny, the three-joint complex concept, the sleep phases and muscular tone. This background knowledge tries to make clear and apprehensible the concept of “the diurnal variation accordion-like phenomenon of wedged intervertebral discs”, which is argued to constitute a key progression factor in IS. This concept seems to be original, existent and it will clinically be very useful for tailoring the treatment of the children suffering IS. The treatment methods currently used to reverse this progression of the IS mechanism are also mentioned. The final great benefit for this group of children will be an unfused spine, as mother nature created it, yet the economies of the national health systems, will be prevented by the high expenditures of traditional surgical treatment, if non operative treatment will properly be applied, based on this concept.

INTRODUCTION

Mechanobiology

Mechanical biology, or the so-called mechanobiology, of the development of skeletal deformity, is an important relatedly novel area of study. Mechanobiology combines biology, engineering, and physics [1]. It is interesting to understand the mechanisms by which cells react to mechanical signals a phenomenon termed mechanotransduction. Mechanotransduction seems to be involved to the development of deformity [2].

Willem Roux,[3], first published on the developmental mechanics of organisms including how mechanical stimuli mediated also on the shaping of muscles and bone. This work inspired the Hueter-Volkman principle [4-7], Pauwel’s theory [8,79] and Wolff’s law [9]. Deposition of new bone is the result of increased loading on bone tissue while decrease in mechanical loading causes resorption of bone tissue, [10].

Connective tissue adaptation, including the development of cartilaginous anlagen into bones, is related to dynamic, intermittent load and stress application, while static stress, acts deleteriously for tissue adaptation, [11]. The architecture

of trabecular bone, the porous bone found in the spine and at articulating joints, provides the requirements for optimal load transfer, by pairing suitable strength and stiffness to minimal weight according to the rules of mathematical design, [9,12-16]. However, it was reported that it is unlikely that the architecture is fully encoded in the genes, [17]. Additionally it is reported that epigenetics play a role in the IS phenotype [18-25]. The answer of how the bone cells are informed and drive the architecture, may be based on the relationship between bone architecture and mechanical usage [26]. While strenuous exercise increases bone mass, [27], disuse, as in microgravity and inactivity, reduces it [28]. It has also been proposed a computational model of the metabolic process in bone, which confirms that cell coupling is governed by feedback from mechanical load transfer [29-31]. The regulatory process that was proposed involves the following hypotheses: a. the mechanical factor that activates response from the external forces to bone metabolism is a typical strain-energy density (SED) rate in the mineralized tissue, b. osteocytes respond to the loading in their local environments by producing a biochemical messenger in proportion to the typical SED rate, c. the biochemical messenger triggered by the osteocytes causes signals to be dissipated through the osteocytic network towards the bone surface, where they create an osteoblast

recruitment stimulus [32], d. to portray resorption in the model, the probability p of osteoclast activation per surface site at any time is considered to be regulated either by the presence of micro-cracks within the bone matrix (hypothesis I) or by disuse (hypothesis II) [33].

FUNDAMENTALS OF THE EMBRYOLOGY AND BIOLOGY OF THE SPINAL COLUMN

Based on this basic embryological development [34], it is clear that any asymmetrical loading on the spine during growth when IS develops, mainly occurs on secondary ossification centers, that is upon the still open ring epiphyses. During growth, if the loading on ring epiphyses is imbalanced or asymmetrical, then a continuous compressive loading decelerates the growth, according to Hueter-Volkman principle, and any intermittent loading promotes the growth, according to Pauwel's law. However, during the period of pubertal growth, any asymmetrical loading will mainly disturb the growth at the secondary growth centers of the vertebrae, that is the two ring epiphyses and the other three secondary ossification centers. The results of Wolff's law will apparently be evident after bone maturation in the spine.

THE INTERVERTEBRAL DISC (IVD) (OR INTERVERTEBRAL FIBROCARILAGE)

The IVD lies between adjacent vertebrae in the vertebral column. Each disc forms a fibrocartilaginous joint, to allow slight movement of the vertebrae, to act as a ligament to hold the vertebrae together, and to function as a shock absorber for the spine. The IVD consists of the annulus fibrosus (AF), and the nucleus pulposus (NP). The NP functions to distribute hydraulic pressure in all directions within each IVD under compressive loads. Among other molecules the NP contains aggrecan, a proteoglycan that aggregates by binding to hyaluronan. Attached to each aggrecan molecule are glycosaminoglycan (GAG), chains of chondroitin sulfate and keratan sulfate. The GAGs play a role in osmotic pressure, resulting in a shift of extracellular fluid from the outside to the inside of the nucleus pulposus. The amount of GAGs (and hence water in the IVD) decreases with age and degeneration, [35-37]. The GAGs imbibe water when they are unloaded and expel it when the disc is loaded. The swelling of IVD correlates directly with GAG content, [38-40]. In IS the IVD is grossly deformed. On the concave side of the IS curve the disc height is markedly reduced, while on the convex side it is increased, so that much of the deformity of scoliosis lies in this change in the disc, [41]. The NP in IS, mainly at the apical but at the neighboring IVDs, migrates to the convex side, as it is surgically confirmed [42]. This migration is also confirmed in MRI studies. It is reported that deterioration of IS has been associated with displacement of the NP towards the convex side, [43,44]. Yet the GAGs composition and content on the concave side of the IVD is different to that on the convex of the NP, [45]. It has been shown experimentally that proteoglycan synthesis and composition may be affected by altered mechanical stresses. Thus, the changes found in the proteoglycan content of the IS discs may result from changed mechanical environment. These changes will also influence disc hydration, [41,46].

THE DIURNAL VARIATION PHENOMENON RELATED TO THE SPINE

Human stature varies throughout the 24-hour period, lengthening when a subject lies down and shortening the upright position. This is termed *diurnal variation*, (DV) [47]. It was suggested, that this DV is due to fluctuation in the water content of the IVD [48].

The DV and changes in body height were studied, using physical measurements and imaging techniques, [49-53]. This DV phenomenon is attributed to the property of proteoglycan macromolecules in the NP. Proteoglycan macromolecules imbibe water when they are not loaded and expel the water under compression loads, due to the so-called Gibbs Donnan effect [54]. Dangerfield et al, 1995, reported that the spinal length changes with respect to upright and recumbent position; these changes are considered to have important clinical significance in the context of 3D IS aetiology, as the spine may be affected in different ways depending on the position adopted by the body' [47]. However, in this report no explanatory mechanism for this consideration was proposed. Czaprowski et al., 2019 reported that body height decreases in children and adolescents with IS during daytime; the height change mostly occurs in the spine and is not related to the curve type or magnitude of IS [55]. However the amount of DV is larger in children as compared to adults [56]. This difference in DV in height between children and adults could be attributed to greater concentrations of purified proteoglycan macromolecules in the NP of children compared with adults. This would allow for more drawing in the water into the IVD during periods of rest, in other words when IVD is not loaded with compressive forces [57].

The risk of progression of the IS is closely related to the longitudinal growth of the spine, the gravity and muscular tone [58,59].

IS aetiology is unclear so far and figuring it out is a great challenge. Up to the present time, the majority of research and reports on pathophysiology of IS are based on IS cases suffering more or less severe deformity when the current indication of treatment is surgery, and not when the curve commences or in mild IS cases, when non-operative treatment is indicated. This discrimination might be significant, because this rather multifactorial condition seems to be dictated from different causes/factors when it commences than when it progresses. There is a view that there are two scoliogenic processes for IS, namely the initiating (or inducing) and those that cause curve progression [20]. These two hypothesized scoliogenic processes for IS, namely the initiating (or inducing) and those that cause curve progression, have been confirmed through imaging studies of the sagittal and frontal views a) in children suffering from mild or moderate AIS referred from school screening programs and b) in severe AIS cases directed to theater. The results are not similar in these two cohorts of IS children. Analyzing the radiographic imaging and the Diers surface topography recordings in children suffering from commencing or mild IS, it was reported that the sagittal profile was not statistically significant different with the peer non-scoliotic children, and not correlated with Cobb angle [60,89]. According to this report's

conclusions, the minor hypokyphosis of the thoracic spine and its minimal differences observed in the studied small IS curves compared with non-scoliotics add to the view that the reduced kyphosis, by facilitating axial rotation, could be viewed as being permissive, rather than as aetiological, in the pathogenesis of IS. This is dissimilar to what was reported elsewhere, that is, that in progressed cases of IS, the sagittal profile is considered as a primary causal factor in IS progression [61-63]. Similarly, in the imaging studies of the coronal deformity, in mild IS curves, when the deformity is initiating, the IVD is found to be wedged, but not the vertebral body. This interesting finding led to the conclusion that the spine initially becomes deformed at the level of the IVD, probably due to the increased plasticity of the IVD, in the way of either torsion or wedging, as an expression of other initiating factors that may result in IS; then, the vertebral bodies are patho-remodeled and deformed [64,65]. This IVD deformation has also been observed and discussed earlier [66,67]. Dissimilarly, in reports concerning progressed and severe cases of IS, the authors suggested that there is an inherent growth bone defect in the vertebrae. It is reported that, although the aetiology of AIS has not been documented, the sagittal profile of the spine is proposed to play a major aetiological role in spinal biomechanics, rotational stability, and the development and progression of spinal deformities [68-73].

THE THREE-JOINT COMPLEX CONCEPT

In 1983, Kirkaldy-Willis described the *intervertebral articulation* as a “**three-joint complex**”, including the disc anteriorly and the two facet joints posteriorly [74], Figure 1.

Sleep phases and muscular tone. The sleep phases are the non-REM and the REM one. The subject can have intense dreams during REM sleep, since the brain is more active. Most of the dreaming occurs during REM sleep, although some can also occur in non-REM sleep. The muscles become temporarily atonic / “paralyzed”, which prevents the subject from acting out his/her dreams. This lack of tone is very important for scolionogenesis and it will be considered below as part of the **diurnal variation “accordion” like phenomenon of wedged intervertebral**

discs: a progression factor in IS. As a person ages, sleeps less of the time in REM sleep. Memory consolidation most likely requires both non-REM and REM sleep. Babies can spend up to 50% of their sleep in the REM stage, compared to only about 20% for adults, [75].

THE HYPOTHESIS/THEORY

Up to this point, we have reviewed some related topics and issues on mechanobiology, mechanotransduction process, some fundamentals of the embryology and biology of the spinal column, details on the intervertebral disc, the DV phenomenon, concepts on IS scolionogenesis, the three-joint complex concept and sleep phases and muscular tone. Based on this review we will describe and analyze the concept of the diurnal variation “accordion”-like phenomenon of wedged intervertebral discs, which is proposed to constitute a key progression factor in idiopathic scoliosis. In Lyon, 2009, a concept was proposed suggesting one mechanism for progression of idiopathic scoliosis (IS) under the title “A comprehensive model of idiopathic scoliosis (IS) progression, based on the patho-biomechanics of the deforming “three joint complex”. This presentation suggested an innovative comprehensive model of IS curve progression, based on IVD diurnal variation and the subsequent patho-biomechanics of the deforming “three joint complex”. So far, only the abstract of the presentation has been published [76]. This report is an enriched, extensive and elaborated analysis of this concept, as it has not been detailed hitherto in the literature.

In the mild IS curve, the imbibed water in the convex-wise migrated NP, the GAGs mainly in the apical IVD, but also in the adjacent to the apex discs, are in a greater amount than in the concave site. This is done due to convex-wise asymmetrical distribution of glycosaminoglycans (GAGs) in NP collagen network type II. This results in an asymmetrical pattern of water distribution and consequently to an asymmetrical swelling of the IVD. Throughout the day and night, due to sustained loading and unloading, the wedged IVDs in the IS patient expel fluid and imbibe it more in the convex side. Owing to the 24h DV, in line with above described increased swelling, the loads to the convex

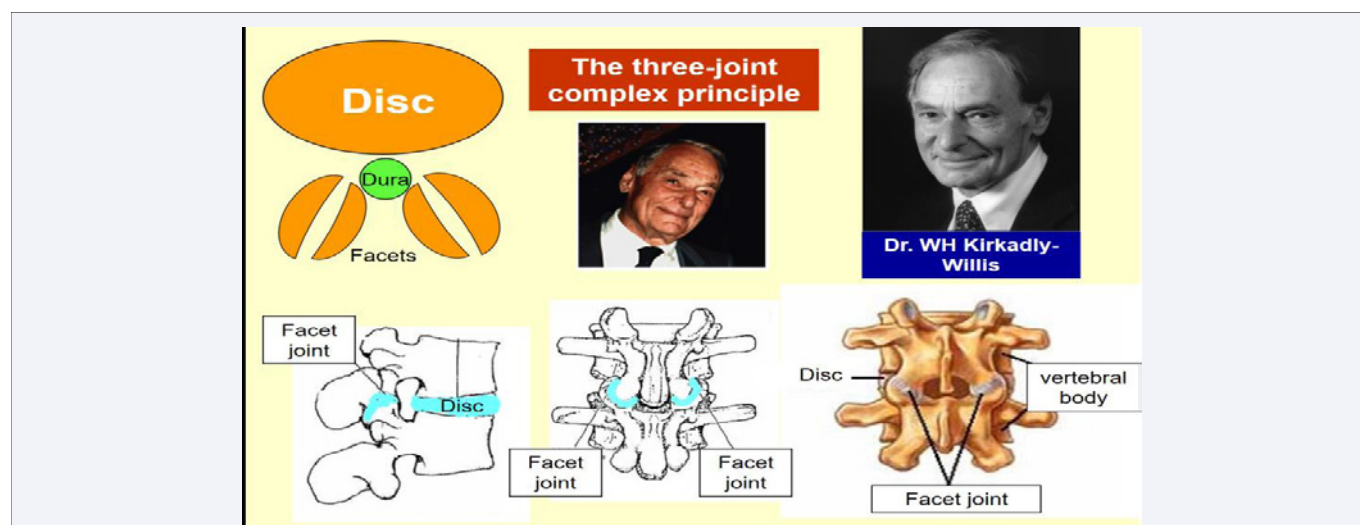


Figure 1 The Three-joint complex principle, including the disc anteriorly and the two facet joints posteriorly.

side of the wedged apical IVD and to the periapical IVDs end plates (ring apophysis), exert asymmetrical convex-wise concentrated cyclical/internment forces. Thus there is greater amount of expansion in this site compared with the convex side. The convex side of the disc sustains a greater amount of cyclic expansion than the concave side. As a result, the convex side end-plates/ring apophyses become intermittently more loaded during the 24-hour period, (Pauwel's law). This intermittent loading of the convex-wise of the IVD, which probably falls within the normal limits of stress and strain, stimulates the growth in the end-plate of the vertebrae convex-wise. However, the concave site of the IS IVD is more likely to be continuously loaded (Hueter-Volkman

law). The continuous compressive forces transmitted to the growth plates/ring plates in the concave site decrease the rate of proliferation of the chondrocytes in the hypertrophic zone. The imposed, convex-wise, asymmetrically concentrated cyclical loads to the adjacent immature vertebral end plates of the spine lead to an asymmetrical growth not only of the vertebral body, but of its posterior elements as well. More specifically, the loading on the two facet-joints is asymmetrical. The asymmetrical increased loading during the day occurs as the wedged IV space narrows due to the expelled water and decreases asymmetrically during the night as the IVD space swells due to the imbibed water. This results in asymmetrical growth, Figures 2, 3 and 4.

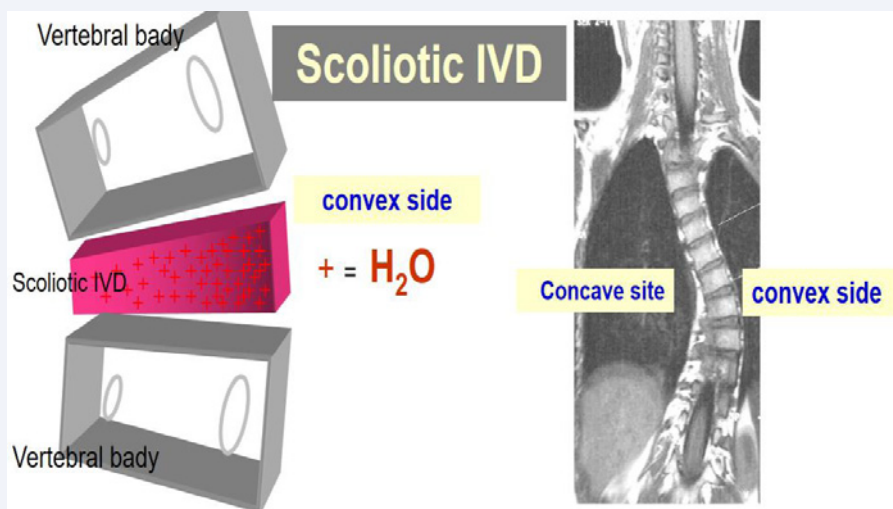


Figure 2 The imbibed water (+ H₂O) mainly in the apical IVD but also in the adjacent discs must be in a greater amount in the convex side than in the concave due to convex-wise asymmetrical distribution of glycosaminoglycans (GAGs) in NP collagen network type II. This results in: 1) asymmetrical pattern of water distribution, 2) Due to DV, asymmetrical convex-wise, concentrated cyclical loads to the IVD during the 24h, the convex side of the wedged IVD sustains greater amount of expansion than the concave side and as a eventual result the vertebra deforms.

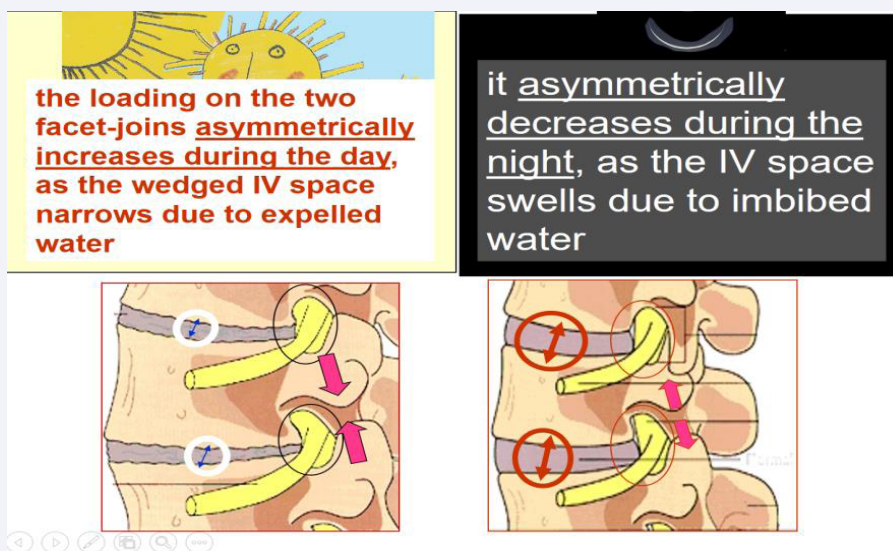


Figure 3 The loading on the two facet-joints and IVDs is asymmetrical. The asymmetrical loading during the day occurs as the wedged IVD space narrows due to the expelled water, and decreases asymmetrically during the night as the IVD space swells due to the imbibed water. This results in asymmetrical growth of vertebral bodies and their posterior elements and also this is reflected in minor fluctuation of Cobb angle during the 24hour period, as was reported in Zetterberg et al 1983, [91], in the younger and more skeletally immature individuals.

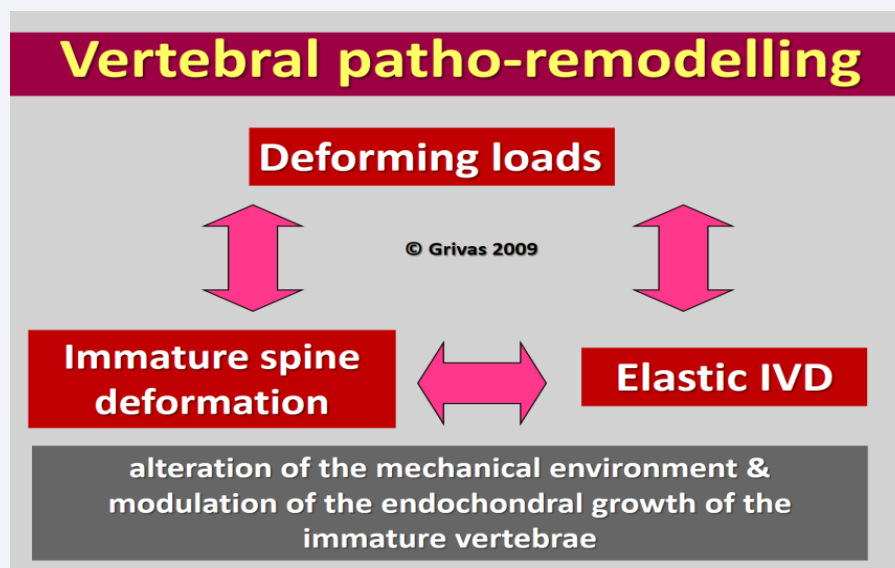


Figure 4 The vicious cycle of patho-remodelling in apical and adjacent vertebrae in a IS curve, due to alteration of the mechanical environment & modulation of the endochondral growth of the immature vertebrae.

The asymmetrical anatomical growth changes in the posterior vertebral elements have been confirmed, see Shea et al, 2004 [77]. This report states that on average, the facets on the convex side have an increased porosity and thinner cortical thickness, and vice versa in the concave site. However, the authors studied surgical cases with more or less developed and mature scoliotic bone; in these cases, it would seem more appropriate to apply Wolff's law. In the mature scoliotic vertebra, in compression loads in facets the cortical thickness increases and the porosity decreases; in tension - (less compression, rather than no tension, would be a more accurate term for the description of the forces) - the cortical thickness decreases and the porosity increases. The authors state that in "scoliotic deformities apply eccentric forces to spinal facets and that the concave and convex portions of the curve are subject to compression and tension forces, respectively. "Similarly, Wang et al., 2011 [78], in relation to the vicious cycle and mechano-transduction in the spine, state that "The progression of skeletal deformity during growth is believed to be governed by laws including the "Hueter-Volkman Law," which states that growth depends on the amount of compression of the growth plate, which can be retarded by increased compression and accelerated by tension."In our opinion, it would be more proper to state that "scoliotic deformities apply eccentric forces to spinal facets and that the concave and convex portions of the curve are subject to compression and "relatively less compression or intermittently more and less compressive forces, respectively." Tension forces can be exerted naturally, if this happens, only during REM sleeping phase, when the atonic phase of the muscles occurs, because tension forces can be exerted on the human body only purposefully or externally or in a no-gravity environment. In all other sleep periods, that is in non-REM phases of sleep but also during daytime in stance posture, only compressive forces are more or less applied, as the muscles always have some degree of tone, no matter if this is strong, mild, or weak. These intermittent, more and less compressive forces, due to the DV phenomenon, apparently according to the Pauwel's law, stimulate growth at the

ring epiphyses. We term the results of these intermittent forces, due to the DV, the "**accordion-like phenomenon**". Therefore, during the 24-hour cycle of a child's life, it is not reasonable to state that there is tension placed on the spine, due to the normal tone of muscles inserted in the vertebra or embracing the spine. And most certainly not while they are sitting or standing. Only when lay down during sleeping, tension may be produced, if not, while in the REM phase of sleep, when muscle tone decreases. Pauwel's law, applied to the growing vertebrae end plates, states that "the intermittent pressure within the normal limits of stress and strain stimulates the growth in the end-plate of a normal vertebra", [79]. The proposed model implies/entails the role of the DV and the asymmetric water distribution in the scoliotic IVD and the subsequent alteration of the mechanical environment of the adjacent vertebral growth plates. Hence, the deformation of the IVD contributes to the progression of IS curves. The eccentric NP of the deformed IVD in the IS spine, through DV in its water concentration, produces an asymmetrically cyclical load during the 24-hour period and an asymmetrical growth of the vertebral body and posterior elements, (Hueter-Volkman and Pauwel's laws). The deformation of the apical IVD and the adjacent to apical discs seems to be an important contributory factor in the progression of a scoliotic curve [80].

Modulation of the IVD mechanical environment by applying corrective forces on the IS curve restores a close-to-normal force application on the vertebral growth plates, and consequently prevents curve progression. The forces are now transmitted evenly to the growth plate and increase the rate of proliferation of chondrocytes at the corrected pressure side, that is the concave side. Application of appropriately directed forces, ideally opposite to the apex of the deformity, likely leads to optimal correction. The wedging of the elastic IVD in the immature IS spine could be reversed by application of corrective forces on it. Reversal of IVD wedging is thus amended into a "corrective", rather than "progressive", factor of the deformity [81]. Through the proposed

model, treatment of progressive IS with braces especially during night time period [90], physiotherapeutic specific scoliosis exercises (PSSE) and growth modulation fusionless surgery by using stapling, growing rods, convex vertebral body tethering techniques or Vertebral growth modulation by posterior dynamic deformity correction devices, could be effective [82-88].

The study of scoliogeny aims to an aetiological treatment, rather than the currently applied symptomatic treatment. Treatment also aims to decrease the possibility of fusion of the spinal column, and to maintain the mobility of the spine, since the human spine is naturally modeled to be articulated and mobile. Additionally, as professor TKF Taylor stated, "the efficacy of early detection and surgical techniques cannot be denied but orthopaedic surgery is not relieved of the responsibility of pursuing the causation and pathogenesis of scoliotic curvature. Spinal fusion for scoliosis cuts across the fundamental principle of orthopaedic surgery – the preservation of musculoskeletal function. Clearly, a sacrifice of spinal mobility is not a final acceptable solution to the malady" [41].

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AUTHOR CONTRIBUTIONS

TBG conceived the concept of "diurnal variation "accordion"-like phenomenon of wedged intervertebral discs: a progression factor in idiopathic scoliosis", conducted the literature review, drafted the text, and fashioned the figures.

REFERENCES

- Wang OJHC, Thampatty BP. An introductory review of cell mechanobiology. *Biomech Model Mechanobiol.* 2006; 5: 1-16.
- Smit TH. Adolescent idiopathic scoliosis: The mechanobiology of differential growth. *JOR Spine.* 2020; e1115.
- Hillen B. Symposium on 'Adaptations of cells and tissues to mechanical stimuli' or 'Roux revisited' held during the Joint Meeting of the Anatomical Society of Great Britain and Ireland, the Anatomical Society of Southern Africa and the Nederlandse Anatomen Vereniging, April 15–18 1998, Rolduc, The Netherlands. *J Anat.* 1999; 194: 321.
- Hueter C. Anatomische Studien an den Extremitätengelenken Neugeborener und Erwachsener. *Archiv für pathologische Anatomie und Physiologie und für klinische Medicin.* 1963; 25: 572-599.
- Hueter C. Anatomische Studien an den Extremitätengelenken Neugeborener und Erwachsener. *Archiv für pathologische Anatomie und Physiologie und für klinische Medicin.* 1863; 26: 484–519.
- Volkman R. Chirurgische Erfahrungen über Knochenverbiegungen und Knochenwachstum. *Archiv für pathologische Anatomie und Physiologie und für klinische Medicin.* 1862; 24: 512-540.
- Volkman R. die Krankheiten der Bewegungsorgane. In: *Handbuch der Allgemeinen und Speciellen Chirurgie*, von Franciscus Pitha und C.A.T. Bilroth, Bd II, Abt 1. Erlangen: Frrdinand Enke. 1869.
- Mau H. Spezifizierung der korrespondierenden Wachstums-Gesetze von Hueter-Volkman und Pauwels (Wachstumsdeformitäten) und ihre Beziehung zu den Belastungsdeformitäten. Specification of the Corresponding Growth Laws of Hueter-Volkman and Pauwels (Growth Deformities) and Their Relationship to Deformities Caused by Stress or Weight. *Z Orthop Unfall.* 1984; 122: 293-298.
- Wolff J. *Das Gesetz der Transformation der Knochen* (Hirchwild, Berlin, 1892); translated as *The Law of Bone Remodeling* (trans. Maquet, P. & Furlong, R.) (Springer, Berlin, 1986).
- Stock JT. Wolff's law (bone functional adaptation) *The International Encyclopedia of Biological Anthropology*. Edited by Wenda Trevathan. 2018 John Wiley & Sons, Inc. Published 2018 by John Wiley & Sons, Inc. 2017.
- Brand RA, Siegler S, Pirani S, Morrison WB, Udupa JK. Cartilage anlagen adapt in response to static deformation. *Medical Hypotheses.* 2006; 66: 653-659.
- Thompson DW. *On Growth and Form* (Cambridge Univ. Press Cambridge, 1919).
- Roesler H. The history of some fundamental concepts in bone biomechanics. *J Biomechanics.* 1987; 20: 1025-1034.
- Cowin SC. Wolff's law of trabecular bone architecture at remodeling equilibrium. *J Biomech Engr.* 1986; 108: 83-88.
- Carter DR, Fyhrie DP, Whalen RT. Trabecular bone density and loading history: Regulation of connective tissue biology by mechanical energy. *J Biomech.* 1987; 20: 785-794.
- Mullender MG, Huiskes R. A proposal for the regulatory mechanism of Wolff's law. *J Orthop Res.* 1995; 13: 503-512.
- Stewart I. *Life's Other Secret* (Allen Lane/Penguin, London, 1998).
- Burwell RG, Dangerfield PH, Moulton A, Grivas TB. Adolescent idiopathic scoliosis (AIS), environment, exposome and epigenetics: A molecular perspective of postnatal normal spinal growth and the etiopathogenesis of AIS with consideration of a network approach and possible implications for medical therapy. *Scoliosis.* 2011, 6: 26.
- Burwell RG, Dangerfield PH, Moulton A, Grivas TB. Adolescent idiopathic scoliosis (AIS), environment, exposome and epigenetics: normal postnatal spinal growth and the etiopathogenesis of AIS. Winter Meeting of the BRITISH ASSOCIATION OF CLINICAL ANATOMISTS (BACA), in association with the Anatomical Society (AS) and the Institute of Anatomical Sciences (IAS), Monday 19th to Wednesday 21st December 2011, Cardiff University, UK
- Burwell RG, Dangerfield PH, Moulton A, Grivas TB, Cheng JCY. Whither the etiopathogenesis (and scoliogeny) of adolescent idiopathic scoliosis? Incorporating presentations on scoliogeny at the 2012 IRSSD and SRS meetings. *Scoliosis.* 2013; 8.
- Grivas TB, Burwell RG, Dangerfield PH, Moulton A. Genetics, epigenetics and the scoliogeny of adolescent idiopathic scoliosis: how much is genetics and how much is it epigenetics as a new paradigm? 2014,
- Grivas TB, Vasiliadis E, Mouzakis V, Mihas C, Koufopoulos G. Association between adolescent idiopathic scoliosis prevalence and age at menarche in different geographic latitudes. *Scoliosis.* 2006; 1: 9.
- Grivas TB, Mihas C, Mazioti C, Sakelaropoulou S, Zisis N, Akriotis N, Burwell RG. Parental Age at Birth Evaluated in Relation to Truncal Back Shape Asymmetry in a Large Sample of Schoolchildren: an Epigenetic Mechanism? E-Poster No: 588. 19th International Meeting on Advanced Spine Techniques (IMAST), Istanbul, Turkey, July 18-21, 2012.
- Grivas TB, Mihas C, Mazioti C, Sakelaropoulou S, Burwell RG. Parental age at birth and truncal back shape asymmetry in school children: Implications for an epigenetic mechanism? 2013.
- Gisselle Pérez-Machado, Ester Berenguer-Pascual, Miquel Bovea-Marco, Pedro Antonio Rubio-Belmar, Eva García-López, María José Garzón, et al. From genetics to epigenetics to unravel the etiology of adolescent idiopathic scoliosis. *Bone.* 2020; 140: 115563.
- Lanyon LE. Using functional loading to influence bone mass and

- architecture: objectives, mechanisms and relationship with estrogen of the mechanically adaptive process in bone. *Bone*. 1996; 18: 37S-43S.
27. Courteix D, Lespessailles E, Peres SL, Obert P, Germain P, Benhamou CL. Effects of physical training on bone mineral density in prepubertal girls: a comparative study between impact-loading and non-impact-loading sports. *Osteopor Int*. 1998; 8: 152-158.
28. Zerwekh JE, Ruml LA, Gottschalk F, Pak CYC. The effects of twelve weeks of bed rest on bone histology, biochemical markers of bone turnover, and calcium homeostasis in eleven normal subjects. *J Bone Min Res*. 1998; 13: 1594-1601.
29. Frost HM. Vital biomechanics: Proposed general concepts for skeletal adaptation to mechanical usage. *Calcif. Tissue Int*. 1987; 45: 145-156.
30. Rodan GA. Mechanical loading, estrogen deficiency, and the coupling of bone formation to bone resorption. *J Bone Miner Res*. 1991; 6: 527-530.
31. Chambers TJ. The direct and indirect effects of estrogen on bone formation. *Adv Organ Biol*. 1998; 5: 627-638.
32. Burger EH, Klein-Nulend J. Mechanotransduction in bone role of the lacuno-canalicular network. *FASEB J*. 1999; 13: S101-S112.
33. Huiskes R, Ruimerman R, van Lenthe GH, Janssen JD. Effects of mechanical forces on maintenance and adaptation of form in trabecular bone. *Nature*. 2000; 405: 704-706.
34. <https://radiopaedia.org/articles/ossification-centres-of-the-vertebral-column>.
35. Roberts S, Evans H, Trivedi J, Menage J. Histology and pathology of the human intervertebral disc. *J Bone Joint Surg Am*. 2006; 88: 10-14.
36. Antoniou J, Steffen T, Nelson F, Winterbottom N, Hollander AP, Poole RA, et al. The human lumbar intervertebral disc: Evidence for changes in the biosynthesis and denaturation of the extracellular matrix with growth, maturation, ageing, and degeneration. *J Clin Investigation*. 1996; 98: 996-1003.
37. Thomas J, Koob, Kathryn G, Vogel. Site-related variations in glycosaminoglycan content and swelling properties of bovine flexor tendon. *J Orthopaedic Res*. 1987; 5.
38. Urban JP, Maroudas A, Bayliss MT, Dillon J. Swelling pressures of proteoglycans at the concentrations found in cartilaginous tissues. *Biorheology*. 1979; 16: 447-464.
39. Urban JPG, McMullin JF. The relationship between disc proteoglycan content and disc height. In *Pathogenesis of Scoliosis. Proceedings of an International Conference*. ed. Jacobs RR, Scoliosis Research Society, Chicago Illinois. 1984; 127-138.
40. Urban JP, Maroudas A. Swelling of the intervertebral disc in vitro. *Conn Tiss. Res*. 1981; 9: 1.
41. Taylor TFK, Ghosh P, Bushell GR. The contribution of the intervertebral disk to the scoliotic deformity. *Clin Orthop*. 1981; 156: 79-90.
42. O'Brien J. Mechanisms of progression in neuromuscular scoliosis, *Proceedings of the Eighth Philip Zorab Scoliosis Symposium*, London, October, (Ed) D. Siegler, D. Harrison, M. Edgar. 1988; 68-69.
43. Toyama Y. An experimental study on the pathology and role of intervertebral discs in the progression and correction of scoliotic deformity. *Nippon Seikeigeka Gakkai Zasshi* 1988; 62: 777-789.
44. Perie D, Curnier D, de Gauzy JS. Correlation between nucleus zone migration within scoliotic intervertebral discs and mechanical properties distribution within scoliotic vertebrae. *Magn Reson Imaging*. 2003; 21: 949-953.
45. Ghosh P, Bushell GR, Taylor TKF, Pearce RH, Grimmer BJ. Distribution of Glycosaminoglycans Across the Normal and the Scoliotic Disc. *Spine*. 1980; 5: 310-317.
46. Jones I, Klämfeldt A, Sandström T. The effect of continuous mechanical pressure upon the turnover of articular cartilage proteoglycans in vitro. *Clin Orthop Relat Res*. 1982; 283-289.
47. Dangerfield P, Roberts N, Walker J, Betal D, Edwards RHT. Investigation of the diurnal variation in the water content of the intervertebral disc using MRI and its implications for scoliosis. In: *The Three Dimensional Analysis of Spinal Deformities*, M. D'Amico et al (Eds.) IOS Press. 1995: 447-451.
48. De Puky P. The Physiological oscillation of the length of the body. *Acta Orthopaedica Scand*. 1935; 6: 338-347.
49. Voss LD, Bailey BJR. Diurnal variation in children: is stretching the answer? *Arch Dis Child*. 1997; 77: 319-322.
50. Adams MA, Dolan P, Hutton WC. Diurnal variations in the stresses on the lumbar spine. *Spine*. 1987; 12: 130-137.
51. Isherwood I, Prendergast DI, Hickey DS, Jenkins JPR. Quantitative analysis of intervertebral disc structure. *Acta Radiol Suppl*. 1987; 369: 492-495.
52. Boos NA, Wallin T, Gbedgbegnon T, Aeebi M, Boesch C. Quantitative MR imaging of lumbar intervertebral discs and vertebral bodies; influence of diurnal water content variations. *Radiology*. 1993; 188: 351-354.
53. Roberts N, Hogg D, Whitehouse GH, Dangerfield P. Quantitative analysis of diurnal variation in volume and water content of lumbar intervertebral discs. *Clin Anat*. 1998; 11: 1-8.
54. Maroudas A and Evans H. A Study of Ionic Equilibria in Cartilage. *Connective Tissue Research*. 1972; 1: 69-17.
55. Czaprowski D, Tyrakowski M, Bloda J, Waś J, Dembińska A, Ewertowska P, Kotwicki T. Diurnal variation of body height in children with idiopathic scoliosis. *J Back and Musculoskeletal Rehabilitation*. 2019; 32: 731-738.
56. Krishan K, Sidhu MC, Kanchan T, Menezes RG, Sen J. Diurnal variation in stature – Is it more in children or adults? *Bioscience Hypotheses*. 2009; 2: 174-175.
57. Jobnstone B, Bayliss MT. The extracellular matrix of the intervertebral disc: proteoglycan biochemistry. In: *Aspden RM, Porter KW. eds. Lumbar spine disorders; current concepts*. Singapore: World Scientific. 1995: 51-62.
58. Escalada F, Marco E, Duarte E, Muniesa JM, Belmonte R, Tejero M, et al. Growth and Curve Stabilization in Girls With Adolescent Idiopathic Scoliosis. *Spine*. 2005; 30: 411-417.
59. Goldberg CJ, Fogarty EE, Moore DP, Dowling FE. Scoliosis and developmental theory: adolescent idiopathic scoliosis. *Spine (Phila Pa 1976)*. 1997; 22: 2228-2237.
60. Grivas TB, Dangas S, Samelis P, Maziotou Ch, Kandris K. Lateral spinal profile in school-screening referrals with and without late onset idiopathic scoliosis 10°-20° *Stud Health Technol Inform*. 2002; 91: 25-31.
61. Millner PA, Dickson RA. Idiopathic scoliosis: biomechanics and biology. *Eur Spine J*. 1996; 5: 362-373.
62. Dickson RA. The aetiology of spinal deformities. *Lancet*. 1988; 1: 1151-1155.
63. Dickson RA. Idiopathic scoliosis: foundation for physiological treatment. *Ann R Coll Surg Engl*. 1987; 69: 89-96.
64. Grivas TB, Vasiliadis E, Malakasis M, Mouzakis V, Segos D. Intervertebral disc biomechanics in the pathogenesis of idiopathic scoliosis. *Stud Health Technol Inform*. 2006; 123: 80-83.

65. Will RE, Stokes IA, Qiu X, Walker MR, Sanders JO. Cobb angle progression in adolescent scoliosis begins at the intervertebral disc. *Spine (Phila Pa 1976)*. 2009; 34: 2782-2786.
66. Trueta J. *Studies of the development and decay of the human frame*. Philadelphia, Saunders 1968.
67. MacEwen GD and Kirsch P. Factors affecting the growth of the vertebral bodies and intervertebral discs. *Scoliosis and Growth*. Ed. Zorab PA, Edinburg. Churchill Livingstone. 1971; 40-46.
68. Adams W. *Lectures on the pathology and treatment of lateral and other forms of curvature of the spine*. London, UK: J & A Churchill. 1882; 69-93.
69. Lorentz A. *Pathologie und Therapie der seitlichen Ruckgratverkrümmungen (scoliosis)*. Pathology and treatment of lateral spinal deformities (scolioses). Vienna, Austria: Alfred Holder. 1886. 294.
70. Nicoladoni C. *Anatomie und Mechanismus der Skoliose*. Anatomy and mechanism of scoliosis. Stuttgart, Germany: Neagele. 1904; 1-79.
71. Dickson RA. The aetiology of spinal deformities. *Lancet*. 1988; 8595: 1151-1155.
72. Castelein RM, van Dieën JH, Smit TH. The role of dorsal shear forces in the pathogenesis of adolescent idiopathic scoliosis—a hypothesis. *Med Hypotheses*. 2005; 3: 501-508.
73. Kouwenhoven JW, Smit TH, van der Veen AJ, et al. Effects of dorsal versus ventral shear loads on the rotational stability of the thoracic spine: a biomechanical porcine and human cadaveric study. *Spine*. 2007; 23: 2545-2550.
74. Yong-Hing K, Kirkaldy-Willis WH. The pathophysiology of degenerative disease of the lumbar spine. *Orthop Clin North Am*. 1983; 14: 491-504.
75. <https://www.ninds.nih.gov/disorders/patient-caregiver-education/understanding-sleep#2>, 9/1/2021
76. Grivas TB, Vasiliadis ES, Triantafyllopoulos G, Kaspiris A. A comprehensive model of idiopathic scoliosis (IS) progression, based on the patho-biomechanics of the deforming “three joint complex” Scoliosis. 2009; 4: 010.
77. Shea KG, Ford T, Bloebaum R, D’Astous J, King H. A Comparison of the Microarchitectural Bone Adaptations of the Concave and Convex Thoracic Spinal Facets in Idiopathic Scoliosis. *J Bone Joint Surg*. 2004; 86: 1000-1006.
78. Wang WJ, Yeung HY, Chu WC, Tang NL, Lee KM, Qiu Y, et al. Top theories for the etiopathogenesis of adolescent idiopathic scoliosis. *J Pediatr Orthop*. 2011; 31: S14-27.
79. Pauwels F. *Biomechanics of the locomotor apparatus: contributions on the functional anatomy of the locomotor apparatus*. Berlin, New York: Springer; 1980.
80. Grivas TB, Vasiliadis E, Malakasis M, Mouzakis V, Segos D. Intervertebral disc biomechanics in the pathogenesis of idiopathic scoliosis. *Stud Health Technol Inform*. 2006; 123: 80-83.
81. Grivas TB, Vasiliadis, Rodopoulos G, Bardakos N. The role of the intervertebral disc in correction of scoliotic curves. A theoretical model of idiopathic scoliosis pathogenesis. *Stud Health Technol Inform*. 2008; 140: 333-336.
82. Roye BD, Simhon ME, Matsumoto H, Bakrania P, Berdishevsky H, Dolan LA, et al. Establishing consensus on the best practice guidelines for the use of bracing in adolescent idiopathic scoliosis. *Spine Deform*. 2020; 8: 597-604.
83. Stefano Negrini, Sabrina Donzelli, Angelo Gabriele Aulisa, Dariusz Czaprowski, Sanja Schreiber, Jean Claude de Mauroy, et al. 2016 SOSORT guidelines: orthopaedic and rehabilitation treatment of idiopathic scoliosis during growth. *Scoliosis Spinal Disord*. 2018; 13: 3.
84. Grivas TB, Webb JK, Burwell RG. Progressive Infantile Idiopathic Scoliosis: A Comparison of Three Methods and the Derotation of a Combined Procedure. 25th Annual Meeting of Scoliosis Research Society, September 23-27, 1990, Hilton Hawaiian Village Hotel, Honolulu, Hawaii
85. Newton PO, Kluck DG, Saito W, Yaszay B, Bartley CE, Bastrom TP. Anterior Spinal Growth Tethering for Skeletally Immature Patients with Scoliosis: A Retrospective Look Two to Four Years Postoperatively. *J Bone Joint Surg Am*. 2018; 100: 1691-1697.
86. Wong HK, Ruiz JNM, Newton PO, Gabriel Liu KP. Non-Fusion Surgical Correction of Thoracic Idiopathic Scoliosis Using a Novel, Braided Vertebral Body Tethering Device: Minimum Follow-up of 4 Years. *JB JS Open Access*. 2019; 4: e0026.
87. Yizhar Floman, Ron El-Hawary, Baron S. Lonner, Randal R. Betz, Uri Arnin. Vertebral growth modulation by posterior dynamic deformity correction device in skeletally immature patients with moderate adolescent idiopathic scoliosis *Spine Deform*. 2021; 9: 149-153.
88. Cuddihy L, Danielsson AJ, Cahill PJ, Samdani AF, Grewal H, Richmond JM, et al. Vertebral Body Stapling versus Bracing for Patients with High-Risk Moderate Idiopathic Scoliosis *Biomed Res Int*. 2015; 2015: 438452.
89. Grivas TB, Vynichakis G, Chandrinou M, Mazioti Ch, Papagianni D, Mamzeli A. Are the scoligenetic changes in spine primary or secondary? Study of the lateral spinal profile in mild and moderate idiopathic scoliosis. Virtual 2021 SOSORT meeting.
90. Grivas TB, Rodopoulos GI, Bardakos NV. Night-time braces for treatment of adolescent idiopathic scoliosis. *Disabil Rehabil Assist Technol*. 2008; 3: 120-129.
91. Zetterberg C, Hansson T, Lidström J, Irstam L, Andersson GBJ. Postural and Time-Dependent Effects on Body Height and Scoliosis Angle in Adolescent Idiopathic Scoliosis, *Acta Orthopaedica Scandinavica*. 1983; 54: 836-840.

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